

CRACK IT

# CRACK-IT Challenge: Improved *in vitro* to *in vivo* extrapolation in chemical safety risk assessment of human systemic toxicity

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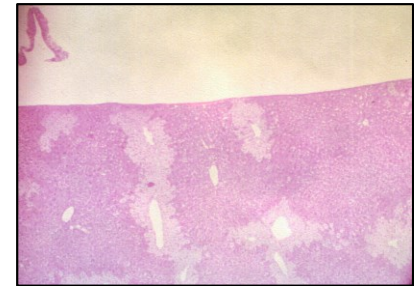


National Centre  
for the Replacement  
Refinement & Reduction  
of Animals in Research

Workshop: Applying exposure science to increase the utility of non-animal data in efficacy and safety testing

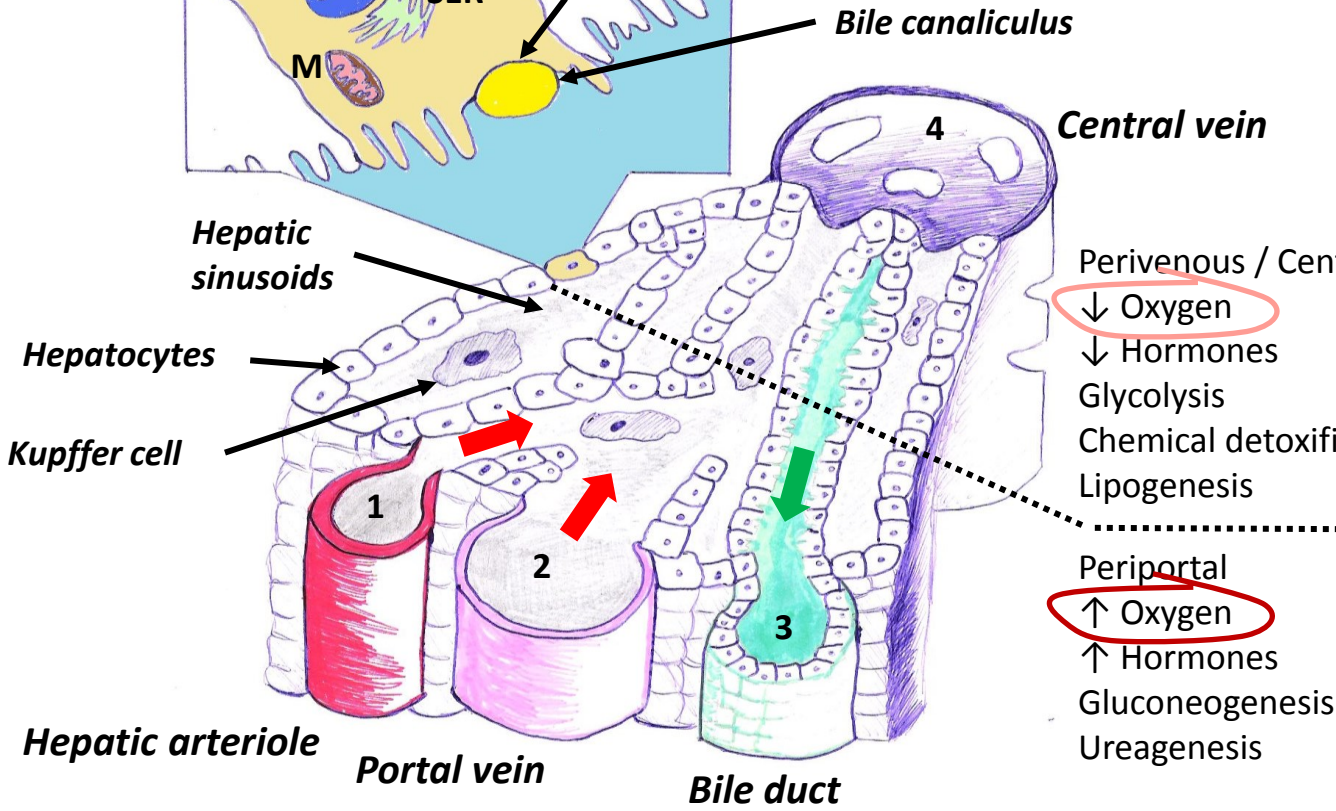
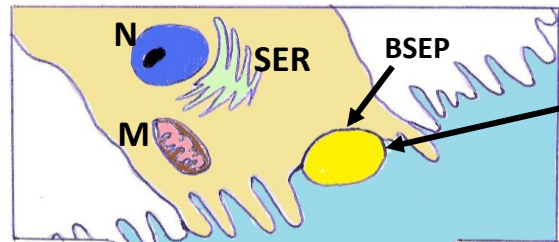
# Drug-Induced Liver Injury

- **Leading cause of acute liver failure<sup>1</sup>**
- **High morbidity & mortality<sup>2</sup>**
- **Main reason for late stage termination or withdrawal<sup>2</sup>**
- **76 drugs found to be significant cause of hepatotoxicity across 3 DILI Registries (US, Sweden, Spain)<sup>3</sup>**
- **Current *in vitro* technologies:**
  - *Physiological gap between incubations and liver*
  - *Lack of physiological integration for amplification/adaptation*
  - *Inability to assess how minor chemical stress leads to major toxicity in some people*

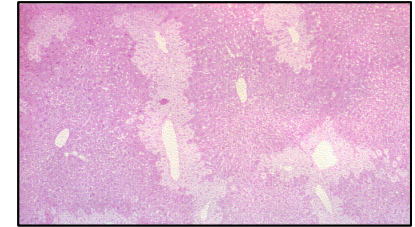


**Require novel translational *in vitro* models of hepatotoxicity**

# Replicating Liver Physiology for toxicology

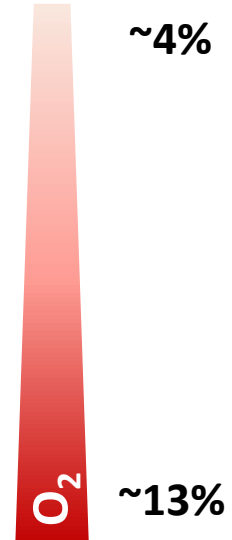


Paracetamol (mouse)

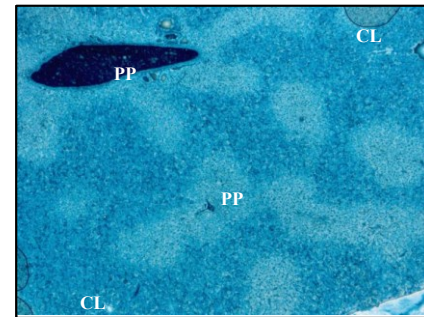


Perivenous / Centrilobular  
 ↓ Oxygen  
 ↓ Hormones  
 Glycolysis  
 Chemical detoxification  
 Lipogenesis

Periportal  
 ↑ Oxygen  
 ↑ Hormones  
 Gluconeogenesis  
 Ureagenesis

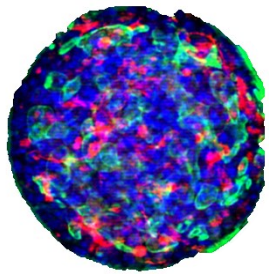
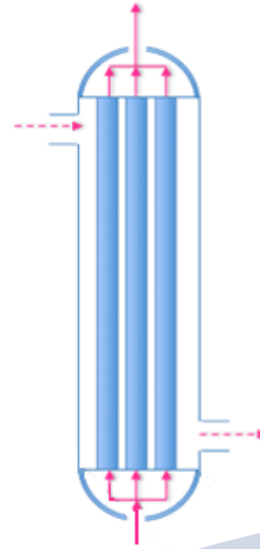


Methapyrilene (rat)



# Mathematical modelling to improve and optimize the design of 3D liver in vitro models

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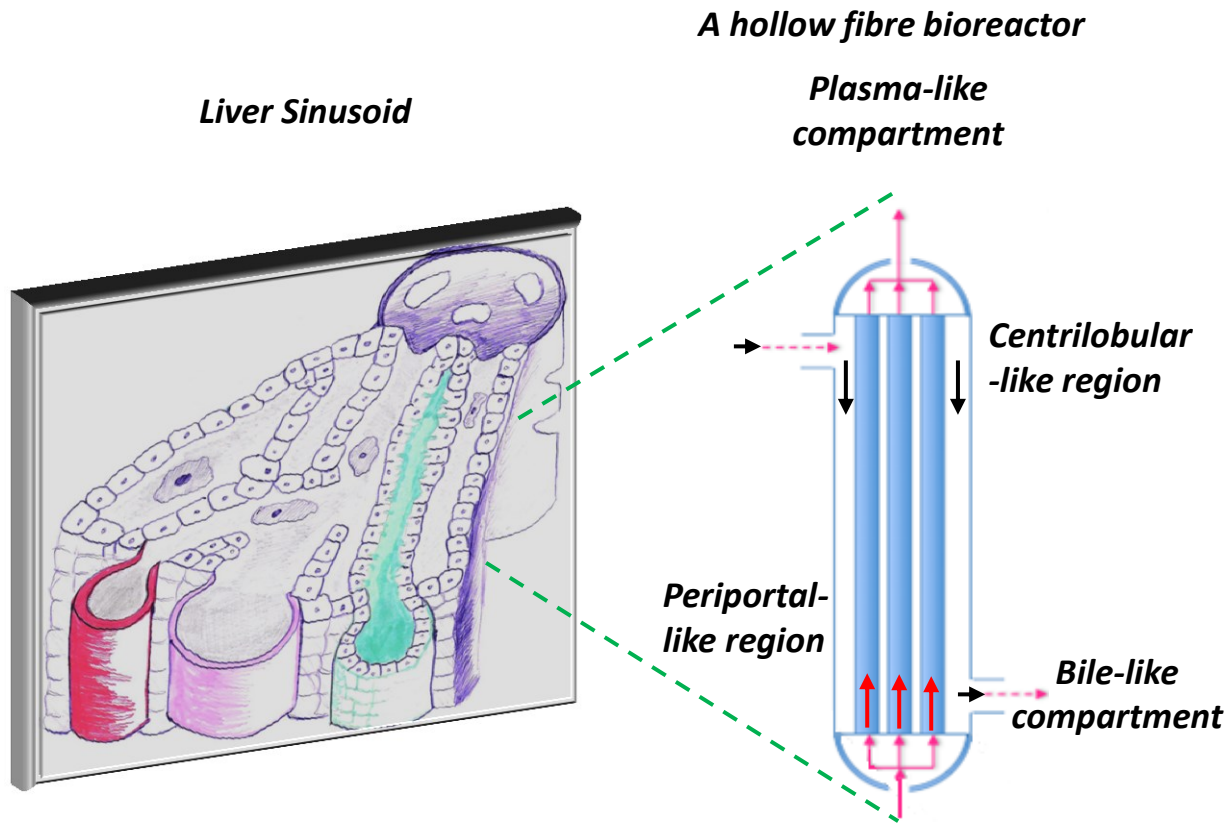


Hepatospheres

Kirkstall Quasi-Vivo

Hollow Fibre Bioreactor

# An *in vitro* hepatic sinusoid: hollow fibre bioreactor



3D cellular scaffolds

Multiple cell-types from same organ

Bioreactor environment allows physiological recapitulation

Hepatocyte zonation

Bile contra-flow

Adaptation to & amplification of response

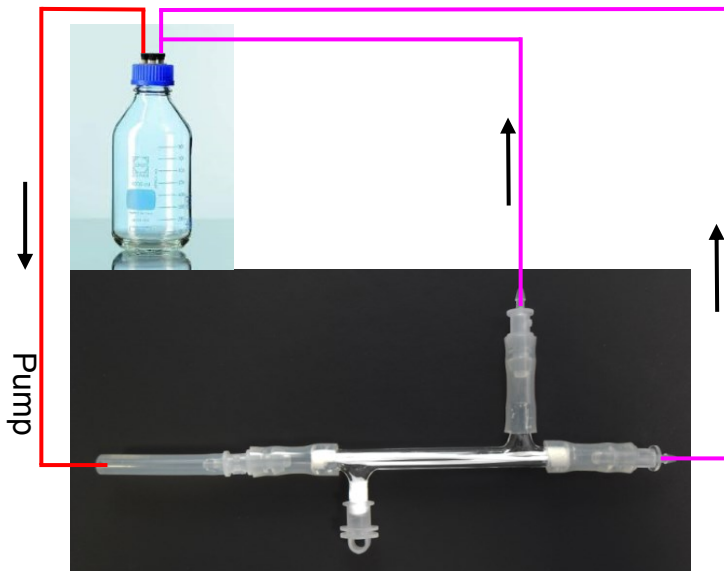
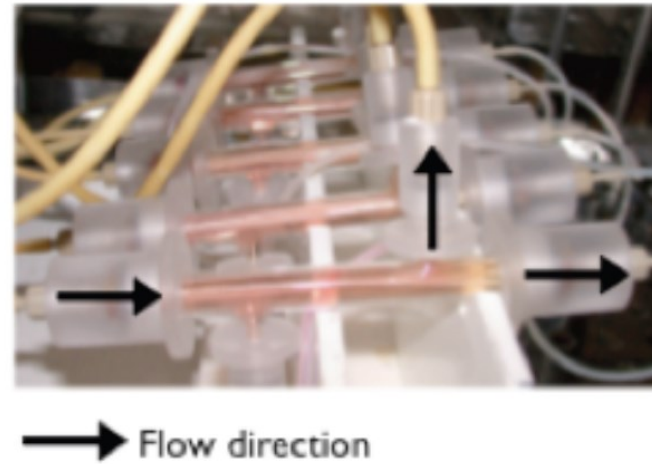
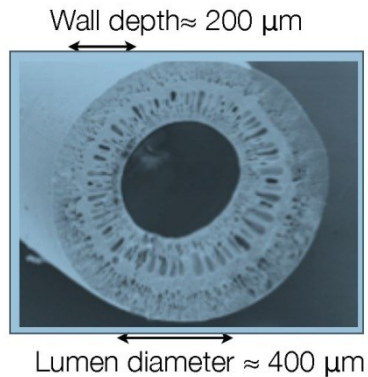
Improved models ADME vs current

Cell number  
Viability  
Morphology

Oxygen level  
Pressures  
Flow rates

Glucose  
Albumin  
Urea  
Glycogen

# Hollow Fibre Bioreactor



## Disadvantages:

- *Fiddly to set-up*
- *Low throughput*

## Advantages:

- *In-vivo like culture system*
  - *Its possible to generate oxygen and nutrient gradients*
- *Cells are shielded from shear stress*
- *Superior mass transport*
- *High cell densities*

# Develop a zonated hepatic hollow fibre bioreactor for chemical safety assessment



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for the Replacement  
Refinement & Reduction  
of Animals in Research

Cathy Vickers



Richard Currie  
Pratibha Mistry



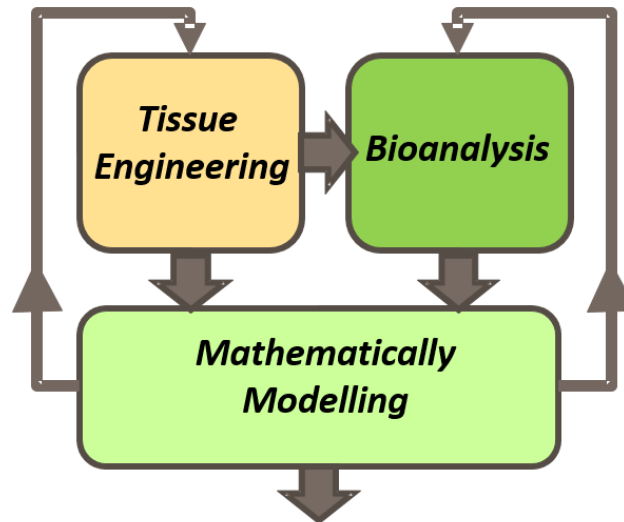
Andrew Scott  
Ian Sorrell



Dominic Williams  
Sophie Regan  
Domingo Salazar



Marianne Ellis  
Mike Storm  
Kim Leutchford



Parveen Sharma  
James Firman



Steve Webb



Rebecca Shipley



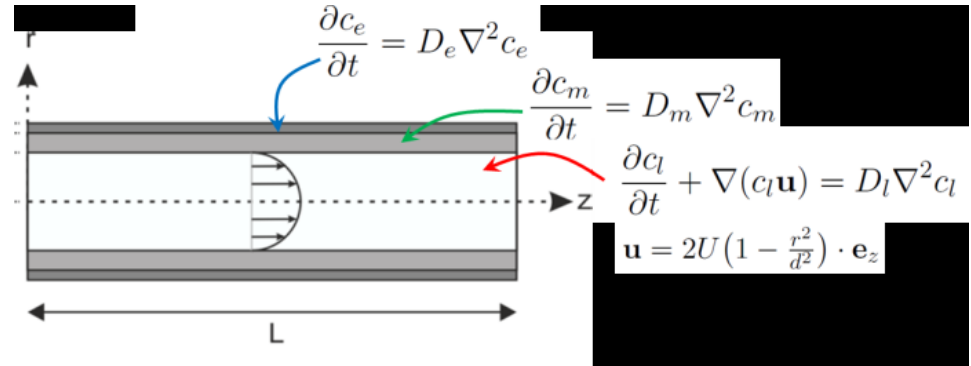
Iain Gardner



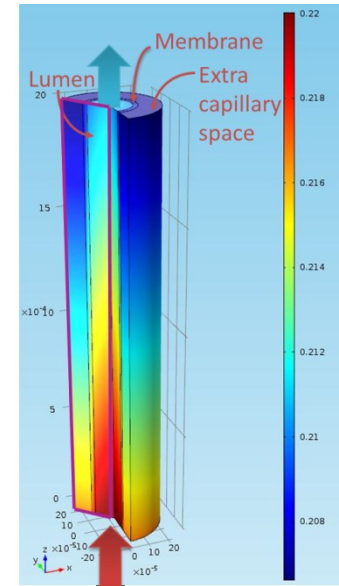
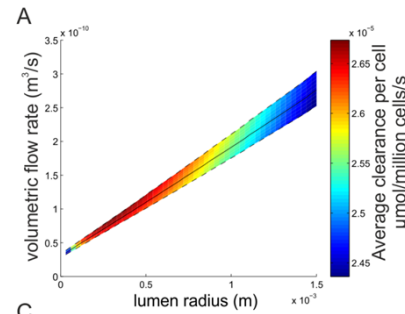
John Ward

# Role of Mathematics

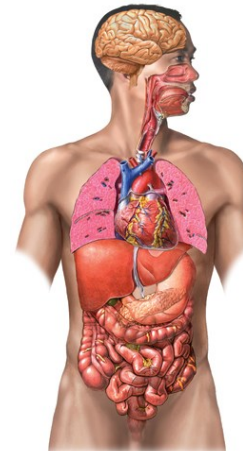
- **Aid design and development**
- **Set operating conditions**
- **Experimental design**



- **Interpret data**
  - *Compare other in vitro systems*
  - *Aid quantification*

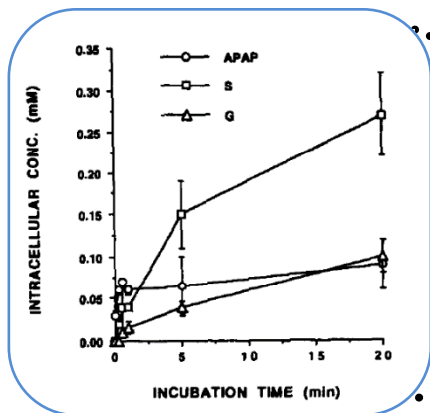


- **Extrapolate from in vitro to in vivo**

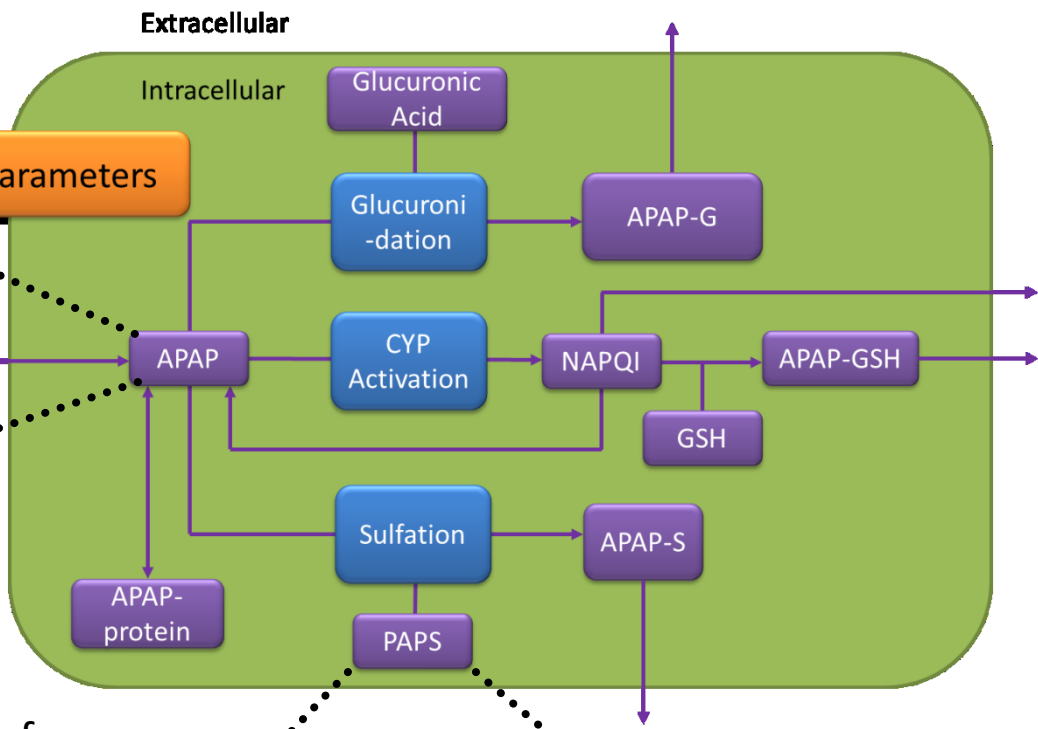




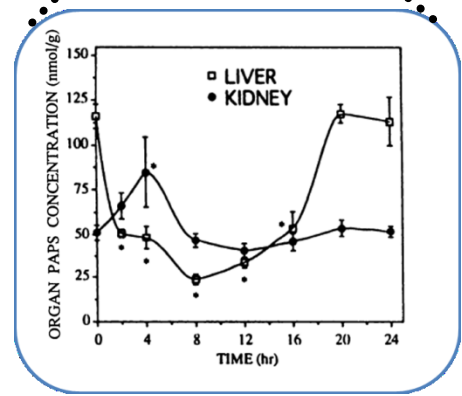
# *In silico* hepatocyte



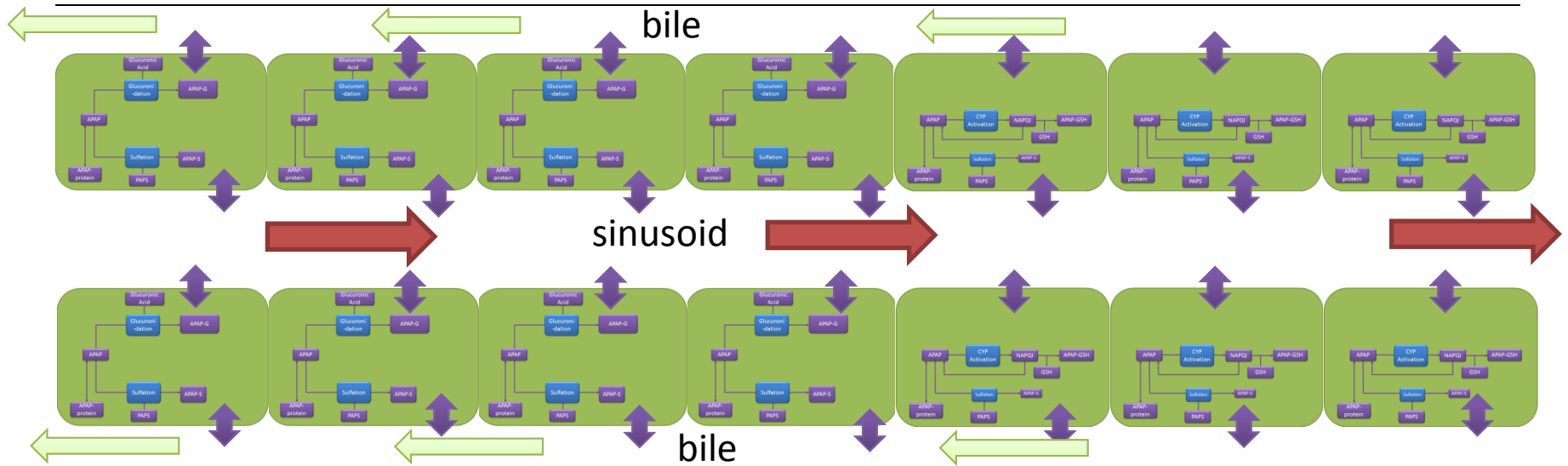
40 parameters



- Parameterized & validated using data from in house and literature
- Modelling directs 'wet-lab' research
- Allows visualization of enzyme capacity



# *In silico* hepatocyte sinusoid



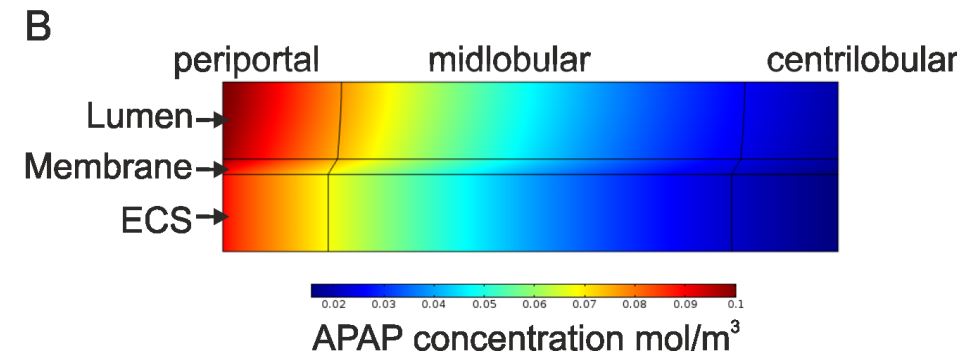
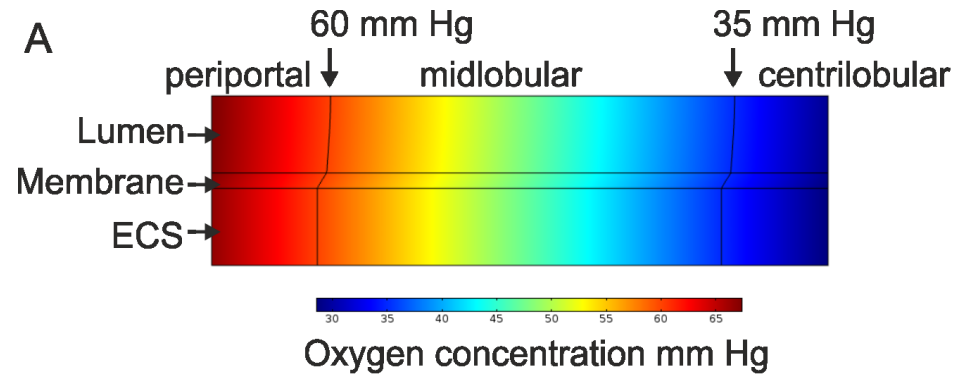
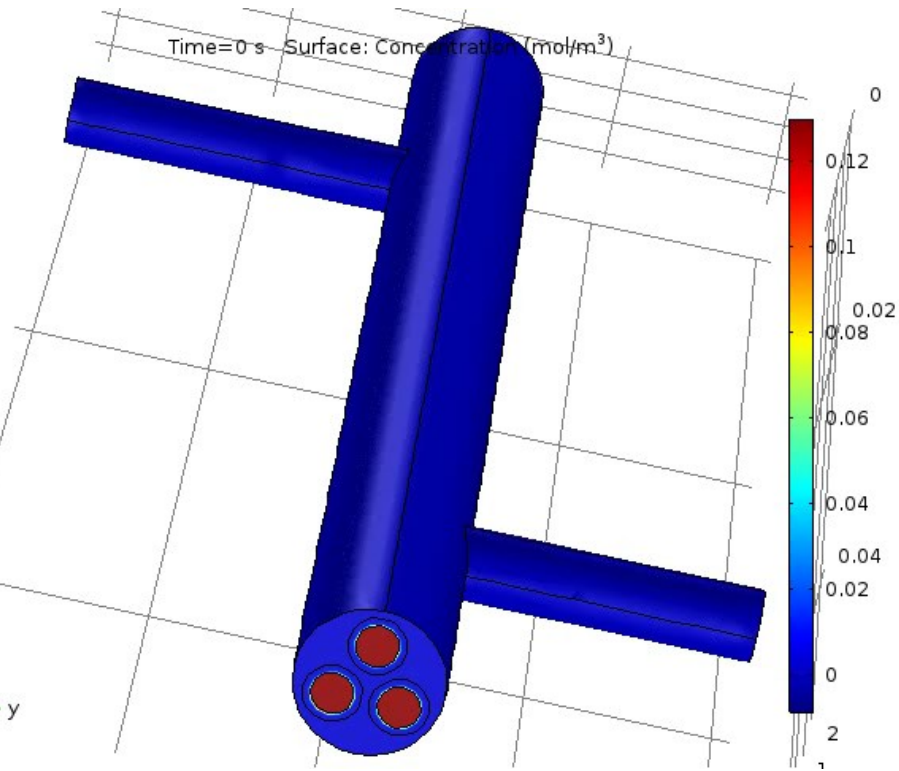
## **HFB Considerations:**

- Physical dimensions
- Membrane properties
- Flow rate
- Inlet oxygen concentration

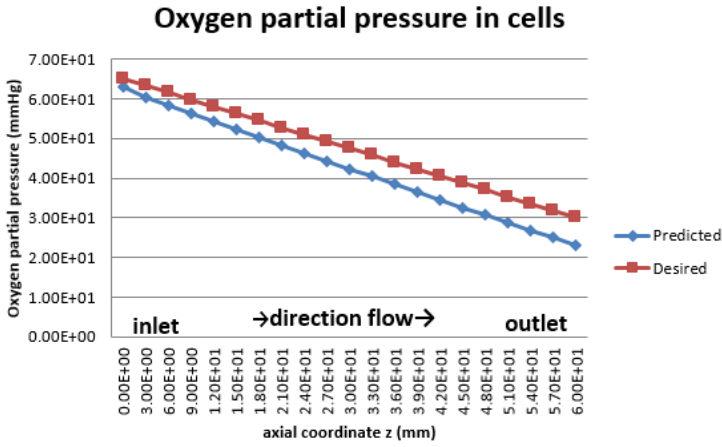
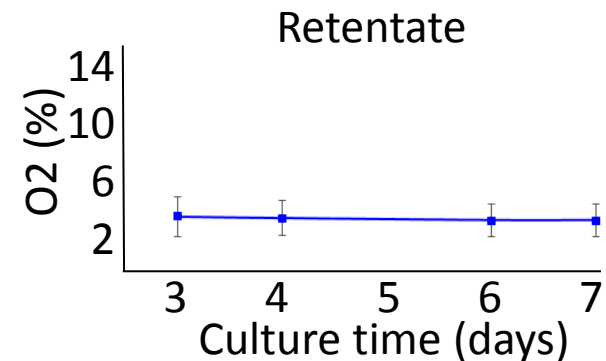
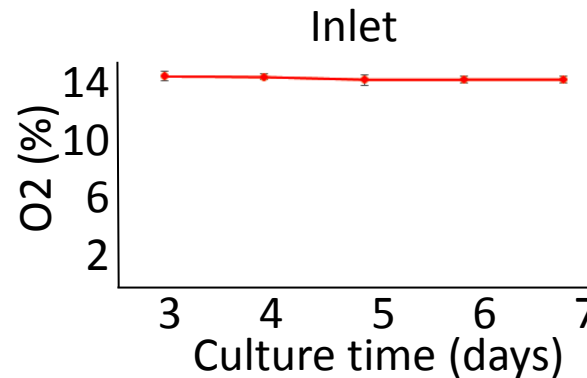
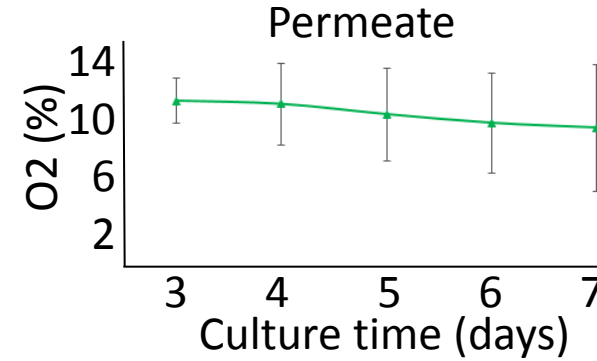
## **Cell considerations:**

- Density
- Oxygen consumption
- Drug uptake/metabolism

# Oxygen and drug transport in HFB



# Mathematical predictions – Oxygen Gradient in HFB

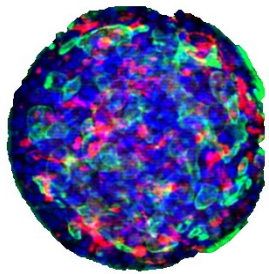
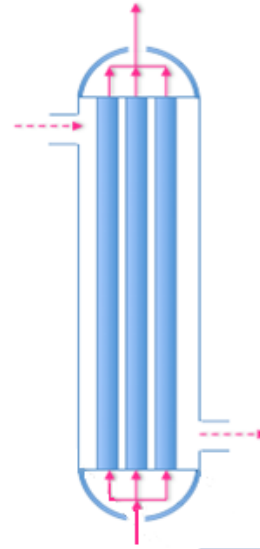


number fibres	3
volumetric flow rate microlitres per hour	400
average single fibre flow (m/s)	1.31E-04
length bioreactor (mm)	60

*HFB set-up optimised via mathematical predictions*

# Mathematical modelling to improve and optimize the design of 3D liver in vitro models

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Hepatospheres

Kirkstall Quasi-Vivo

Hollow Fibre Bioreactor



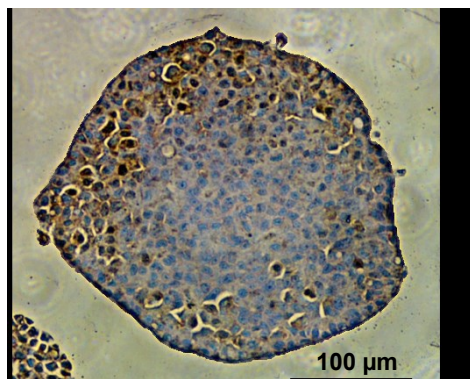
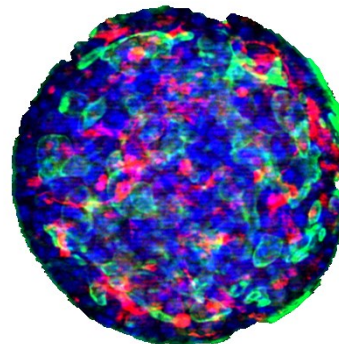
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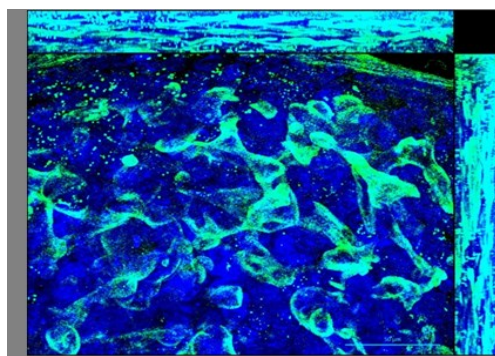
### Characterization of a functional C3A liver spheroid model†

Cite this: DOI: 10.1039/c6tx00101g

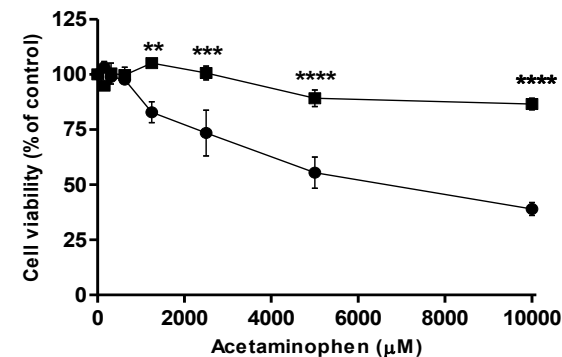
Harriet Gaskell,<sup>ab</sup> Parveen Sharma,<sup>ab</sup> Helen E. Colley,<sup>c</sup> Craig  
Dominic P. Williams<sup>b</sup> and Steven D. Webb<sup>d</sup>



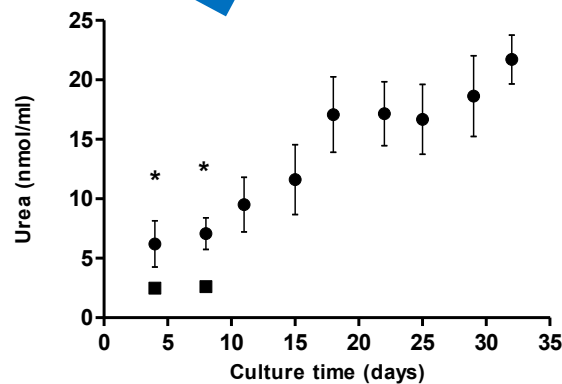
Zonation



Polarisation



Sensitivity to hepatotoxins



Liver-specific function

# Ingredients for a mathematical model



## Maximum O<sub>2</sub> consumption rates:

Fresh human Hep:

$$V_{max} = 7.8 \times 10^{-3} \text{ mol m}^{-3} \text{ s}^{-1}$$

HepG2/C3A:

$$V_{max} = 19.6 \times 10^{-3} \text{ mol m}^{-3} \text{ s}^{-1}$$

## Half maximal O<sub>2</sub> concentration:

$$K_m = 6.24 \times 10^{-3} \text{ mol m}^{-3}$$

## Seahorse Technology

- Monitors OCR and ECAR in live cells
- OCR: oxygen consumption rate (*OXPHOS*)
- ECAR: extracellular acidification rate (*glycolysis*)



Amy Chadwick & Laleh Kamalian



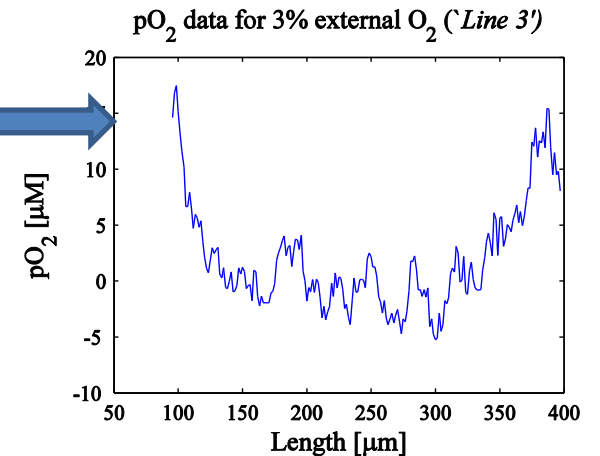
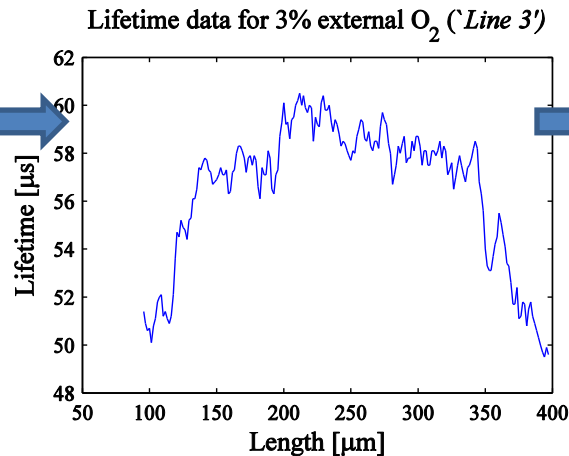
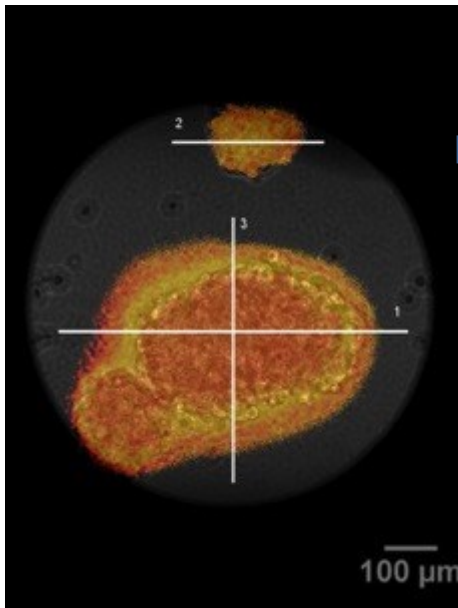
# Ingredients for a mathematical model

## FLIM imaging technique

Intracellularly loaded nanoprobe emits phosphorescence that decays in the presence of oxygen.



**Greater lifetime value  
= lower decay rate  
= less oxygen.**



HeLa cells





# Ingredients for a mathematical model

Time equilibrium system,  
spherical coordinates and  
radial symmetry:

$C$  : Oxygen concentration  
 $D_1, D_2$  : Diffusion inside/outside the spheroid  
 $V_{max}$  : Max consumption rate (constant)  
 $K_m$  : Half maximal concentration.

## INSIDE the Sphere

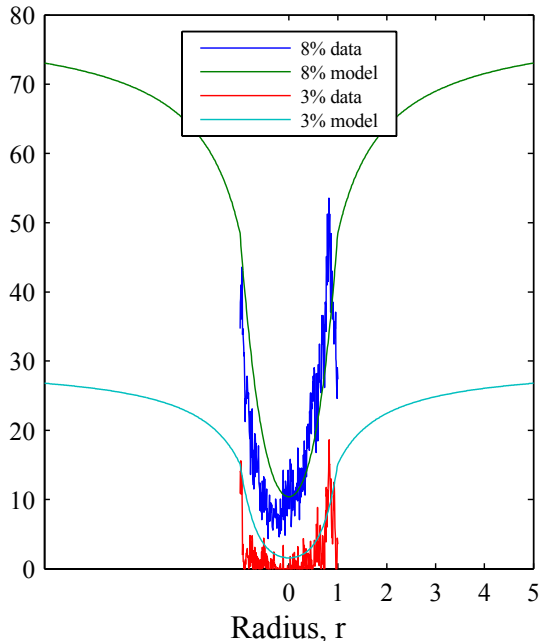
$$D_1 \nabla^2 C - \frac{V_{max} C}{C + K_m} = 0 \quad r \leq R,$$

$$\frac{\partial C}{\partial r} = 0, \quad r = 0.$$

## OUTSIDE the Sphere

$$D_2 \nabla^2 C = 0 \quad \infty \geq r \geq R,$$

$$C \rightarrow C_\infty, \quad r \rightarrow \infty.$$



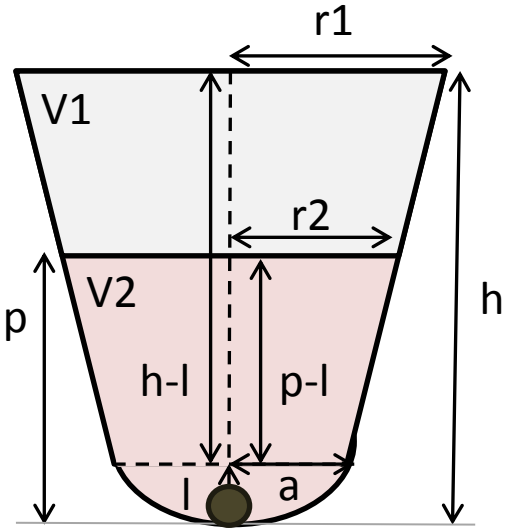
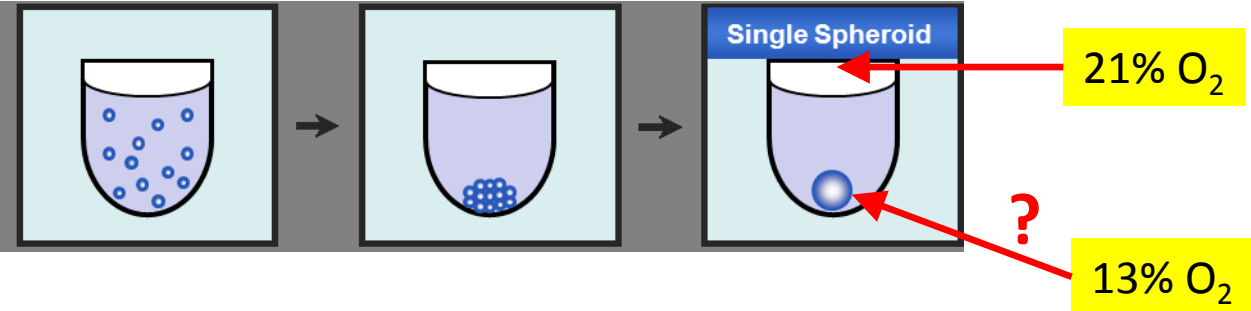
$C_\infty = 3\% O_2$   
 $C_\infty = 8\% O_2$



**DIFFUSION RATE INSIDE THE SPHEROID:**  
 $D_1 = 3.84 \text{ to } 4.23 \times 10^4 \mu\text{m}^2 \text{min}^{-1}$



# Ingredients for a mathematical model



V1	Working vol per well	360ml
V2	Media vol	100ml
r1	Well radius @ top	3.429mm
h	Depth of well	11.303mm
a	Well radius @ bottom	3.175mm
l	Spherical cap height	1.6mm
r2	Media radius @ top	3.2338mm
p	Media depth	3.848mm

# Ingredients for a mathematical model

Time equilibrium system, cylindrical coordinates and radial symmetry,  $C(r,z)$ :

$$0 = \frac{D_2}{r} \frac{\partial}{\partial r} \left( r \frac{\partial C}{\partial r} \right) + D_2 \frac{\partial^2 C}{\partial z^2},$$

*O2 diffusion in media*

**DIFFUSION RATE OUTSIDE SPHEROID:**  
 $D_2 = 1.15 \text{ to } 1.28 \times 10^5 \mu\text{m}^2\text{min}^{-1}$

*Diffusion rate determined from exp fitting by Joe Leedale in (2014), Math BioSci, 258:33-43*

$$0 = \frac{D_1}{r} \frac{\partial}{\partial r} \left( r \frac{\partial C}{\partial r} \right) + D_1 \frac{\partial^2 C}{\partial z^2} - \frac{V_{\max} C}{K_m + C},$$

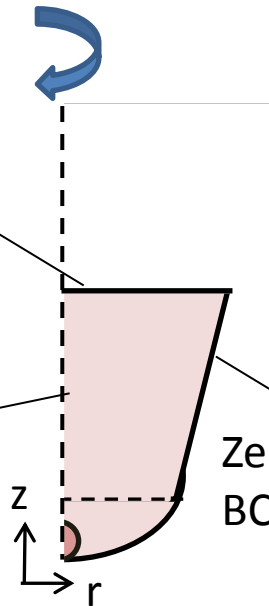
*O2 diffusion and consumption by cells inside spheroid*

axisymmetric

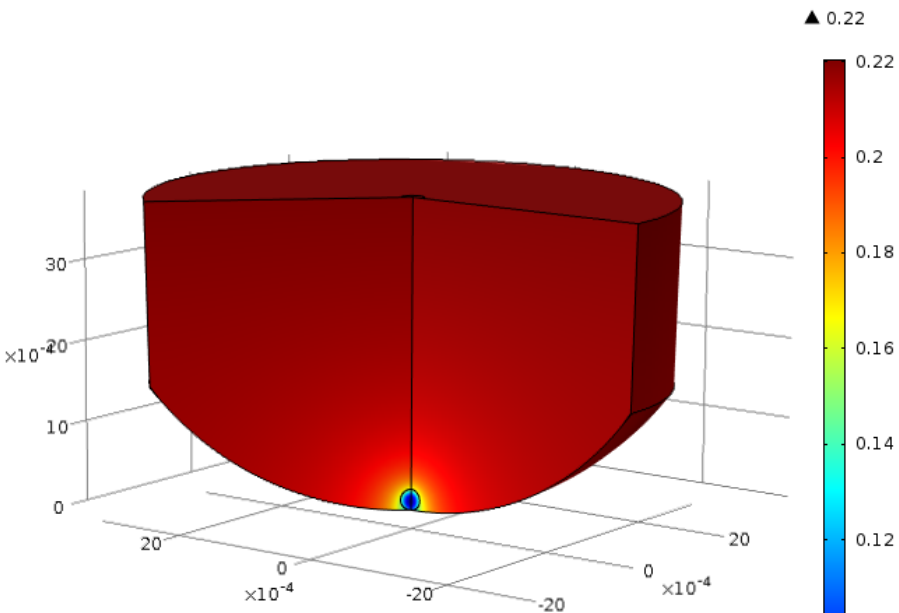
Dirichlet BC:  
 $C=C_0=21\% \text{ O}_2$

IC:  $C=C_0$

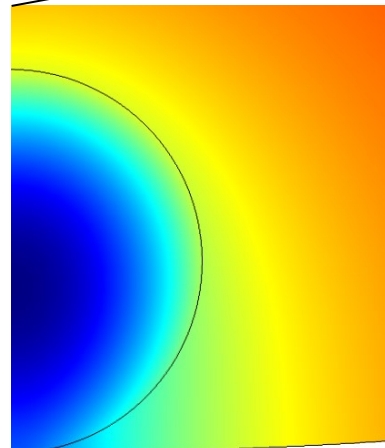
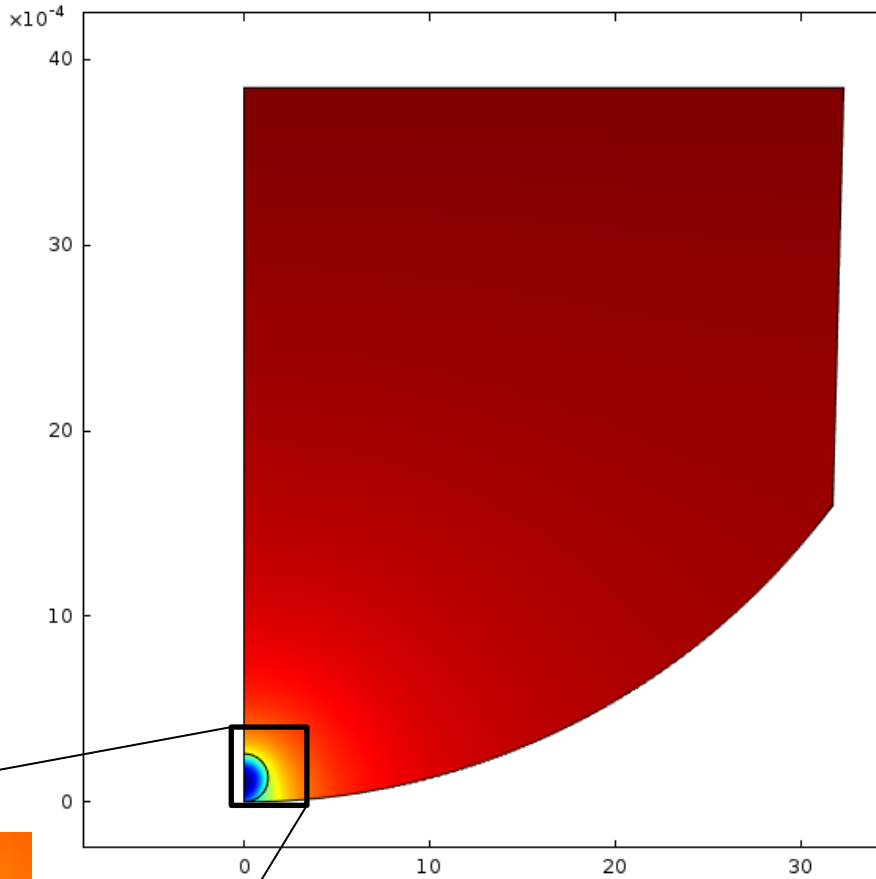
Zero flux BCs



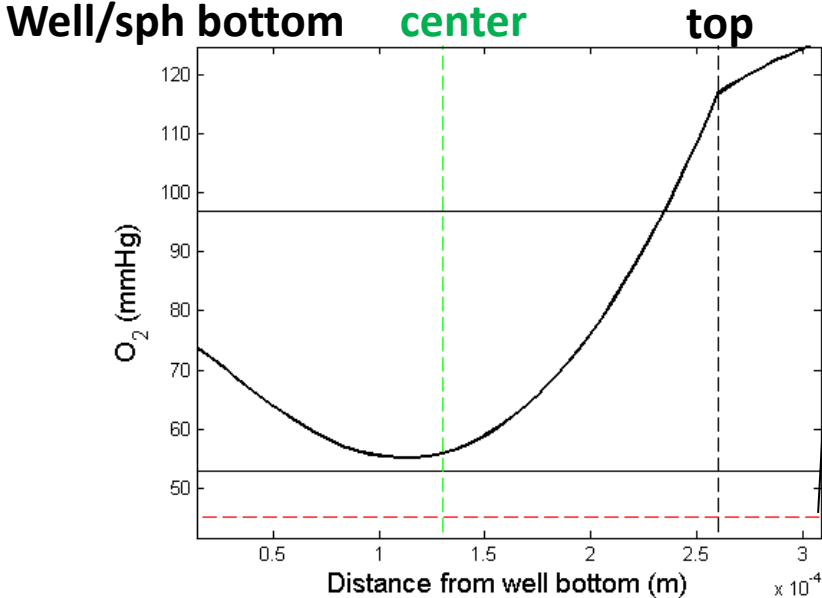
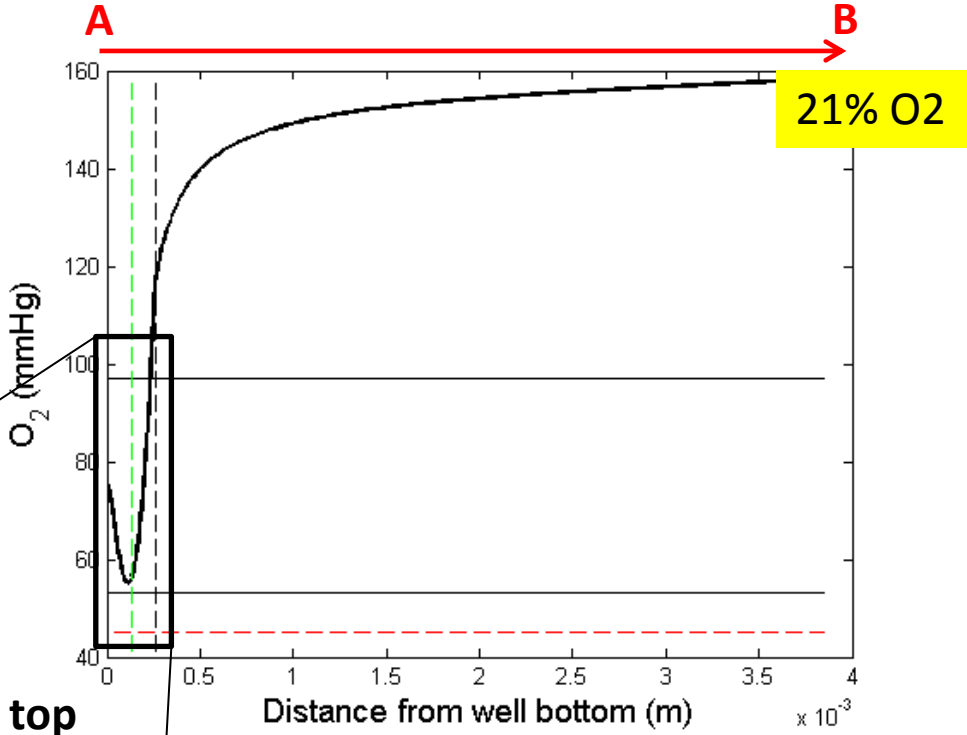
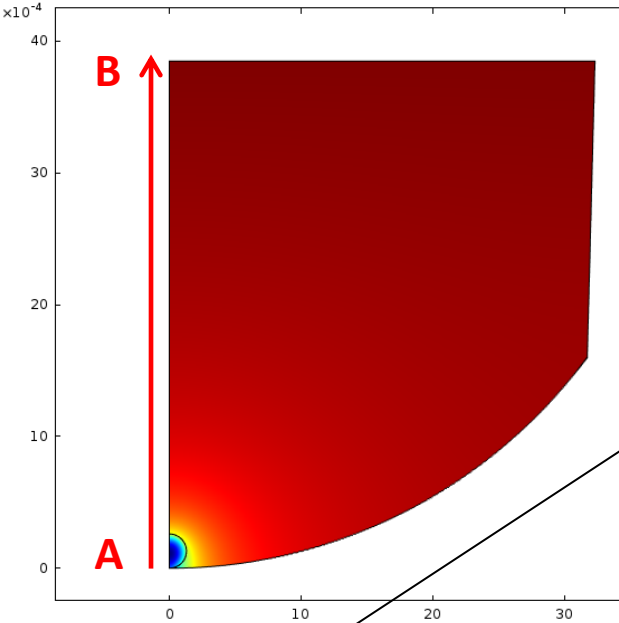
# Model predictions



V2=Media vol=100 $\mu$ l,  
Spheroid radius 130 $\mu$ m  
HepG2/C3A cells



# Model predictions

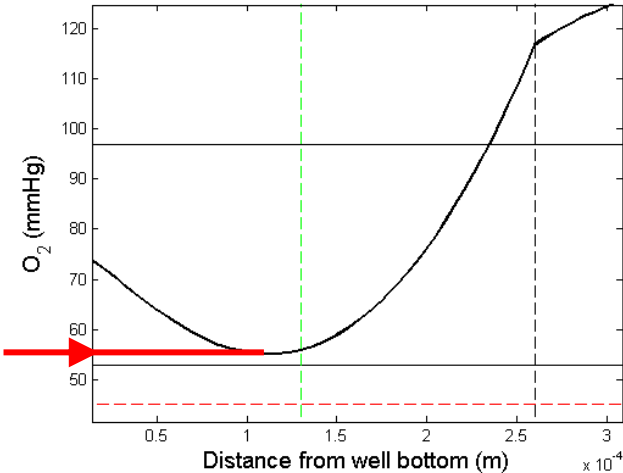
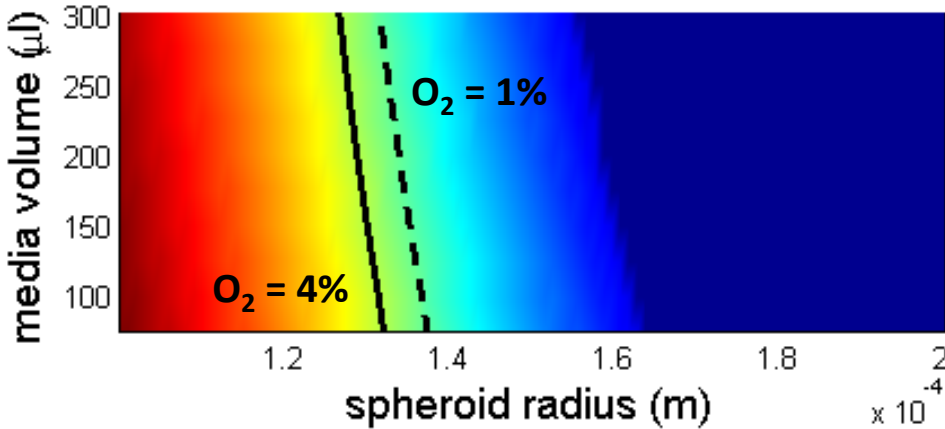
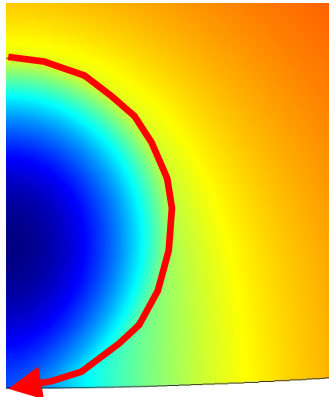
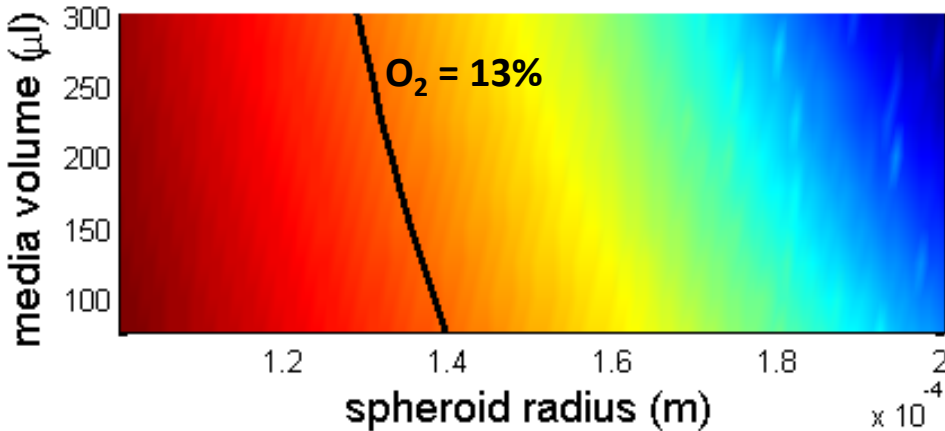


Hepatic portal vein O<sub>2</sub> = 13%

Central vein O<sub>2</sub> = 4%

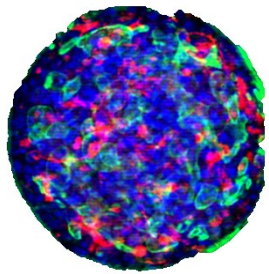
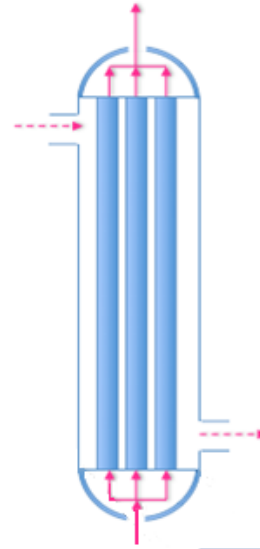
Hypoxia O<sub>2</sub> = 1%

# Model predictions: assay sensitivity



# Mathematical modelling to improve and optimize the design of 3D liver in vitro models

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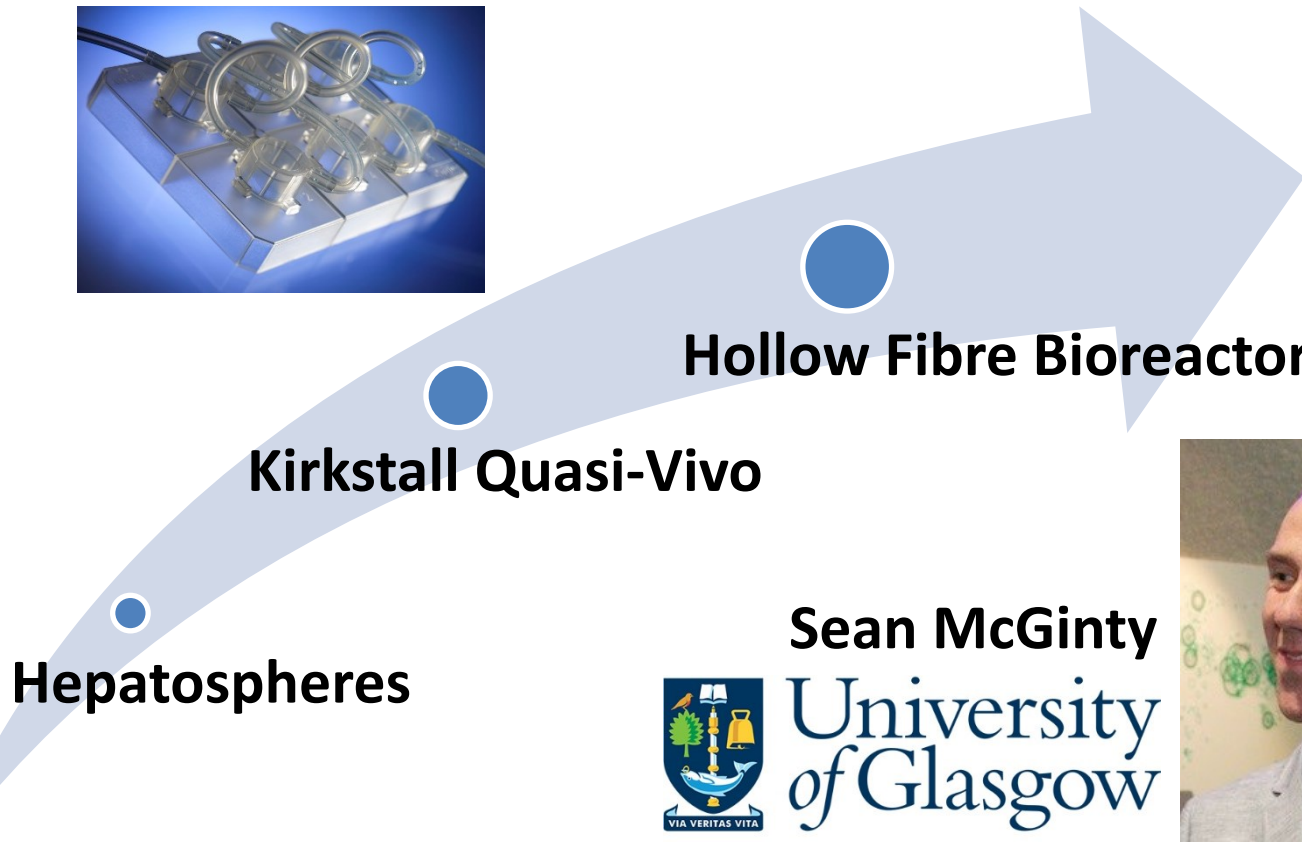
Hepatospheres

Kirkstall Quasi-Vivo

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# Mathematical modelling to improve and optimize the design of 3D liver in vitro models

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Hepatospheres

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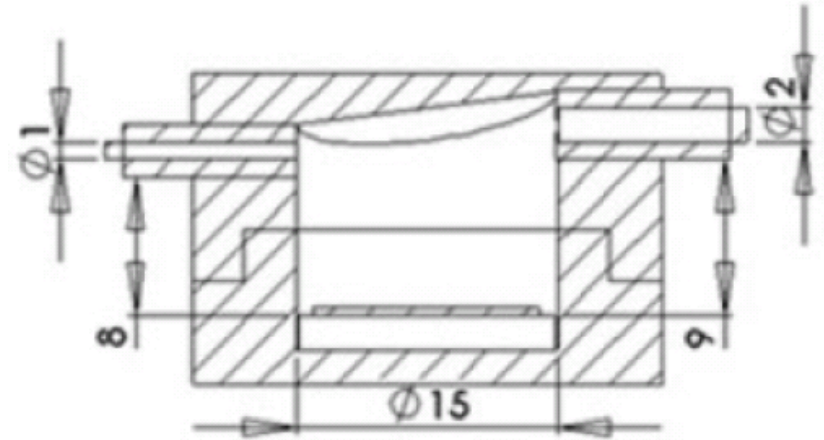


Sean McGinty  
University  
of Glasgow





# Mathematical modelling of the Kirkstall Quasi-Vivo system: QV900



Navier-Stokes equations for the fluid and a convection-diffusion equation for the oxygen concentration:

Boundary conditions:

Inlet: constant concentration

Outlet: normal flux

Zero flux conditions everywhere else

A monolayer of cells is included at the lower boundary. Oxygen obeys a reaction-diffusion model:

$$\nabla \cdot \mathbf{u} = 0$$

$$\rho \frac{\partial \mathbf{u}}{\partial t} + \rho(\mathbf{u} \cdot \nabla) \mathbf{u} = -\nabla p + \mu \nabla^2 \mathbf{u}$$

$$\frac{\partial c}{\partial t} + (\mathbf{u} \cdot \nabla) c = D \nabla^2 c$$

$u$ =flow velocity,  $\rho$ =(const) fluid density,  $p$ =pressure,  $\mu$ =dynamic viscosity,  $c$ =O<sub>2</sub> conc,  $D$ =diff coeff in fluid.

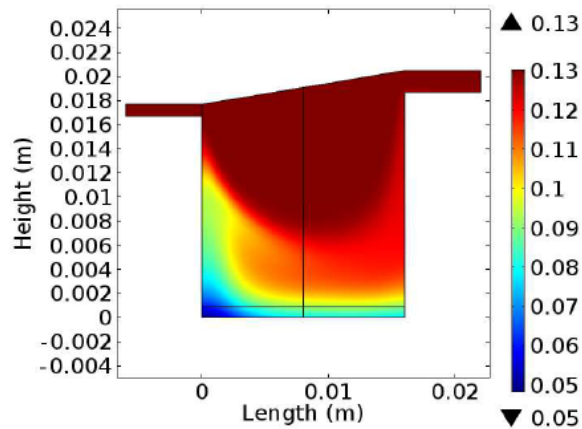
$$\frac{\partial c}{\partial t} = D_g \nabla^2 c - \frac{V_{max} c}{K_m + c}$$

$V_{max}$ =max cell O<sub>2</sub> consumption rate,  $K_m$ =half maximal O<sub>2</sub> conc,  $D_g$ =diff coeff in cell layer.

# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

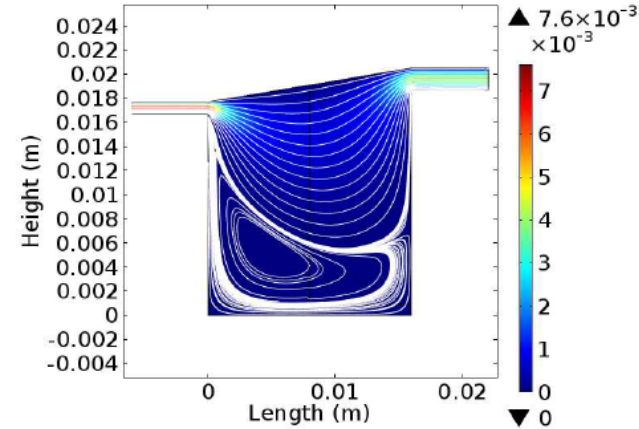
COMSOL 5.0.0.244

Oxygen concentration profile in the chamber (mol/m<sup>3</sup>)



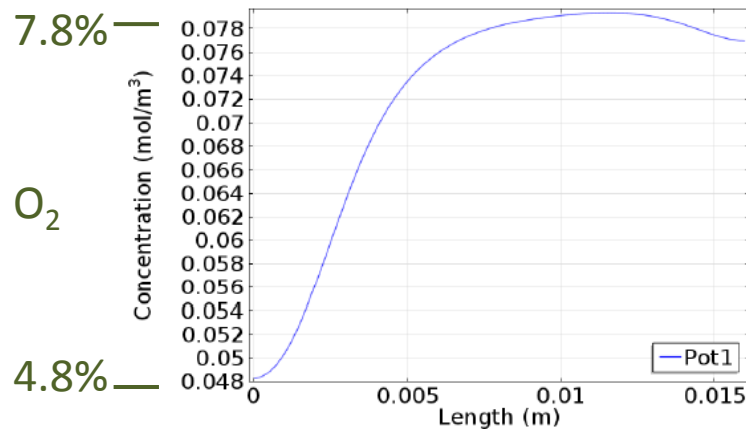
COMSOL 5.0.0.244

Fluid velocity (m/s) and streamlines in the chamber



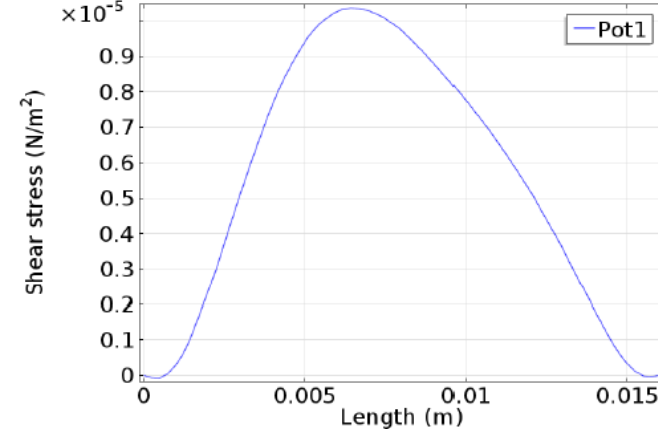
COMSOL 5.0.1.276

Oxygen concentration at cell surface



COMSOL 5.0.1.276

Shear stress at cell surface




Result for Q = 180uL/min. **Top left:** O<sub>2</sub> concentration profile. **Top right:** Flow profile. **Bottom left:** O<sub>2</sub> concentration at the cell surface. **Bottom right:** Shear stress at the cell surface.

# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system



- **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer in a single pot?

- **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer in a single pot? 
- Explored flow rates ranging from 60-1000ul/min.
- Gives O<sub>2</sub> ranges from 3.9%-6.9% to 10.4%-12.2%.
- Shear stress ranges from 1e-5 to 7e-4 N/m<sup>2</sup>
- Increasing height of cells in pots increases min & max O<sub>2</sub> as well as shear stress.

# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer  
in a single pot?



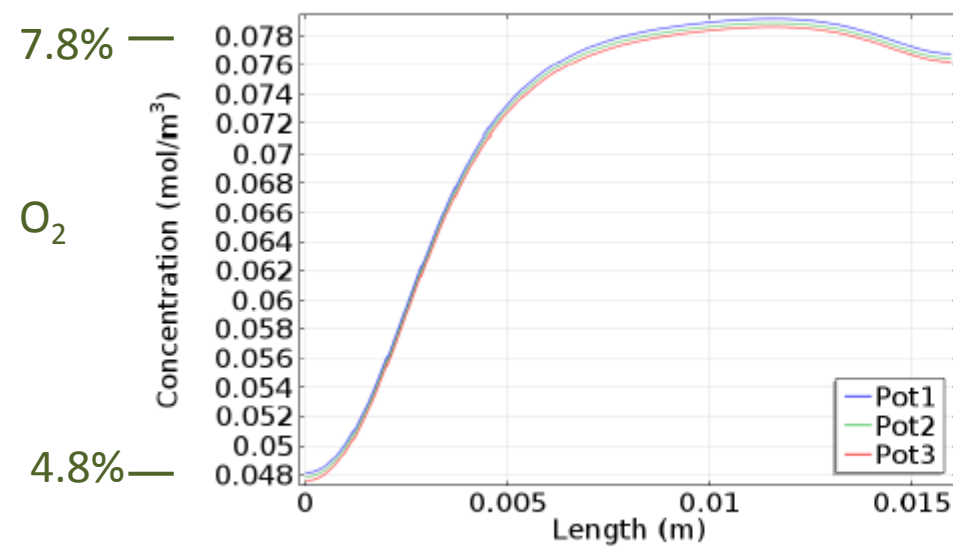
➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer  
across multiple pots?



# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

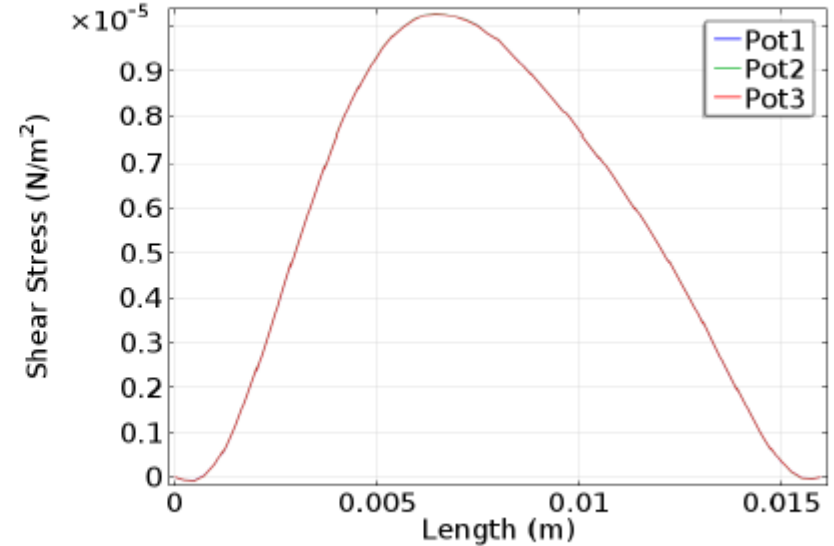
COMSOL 5.0.0.244

Oxygen concentration at cell surface





COMSOL 5.0.0.244

Shear stress at cell surface




Result for  $Q = 180 \mu\text{L}/\text{min}$ . **Left:**  $\text{O}_2$  concentration at the cell surface. **Right:** Shear stress at the cell surface.


# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

- **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer in a single pot? 
- **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer across multiple pots? 
  - O<sub>2</sub> profiles, shear stress very similar in each chamber.



# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

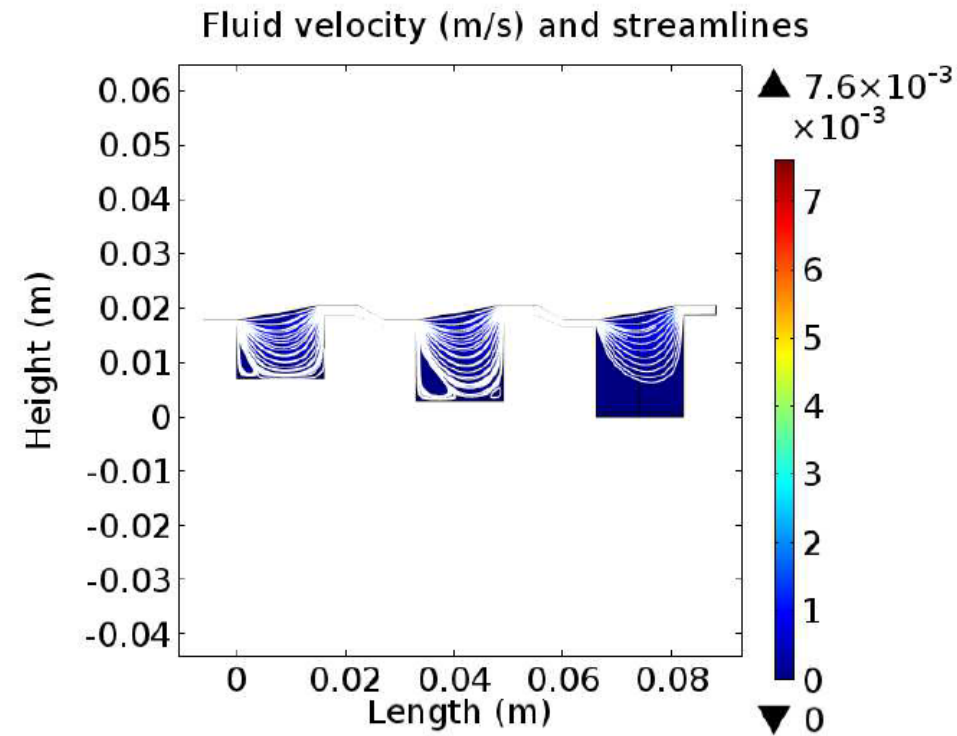
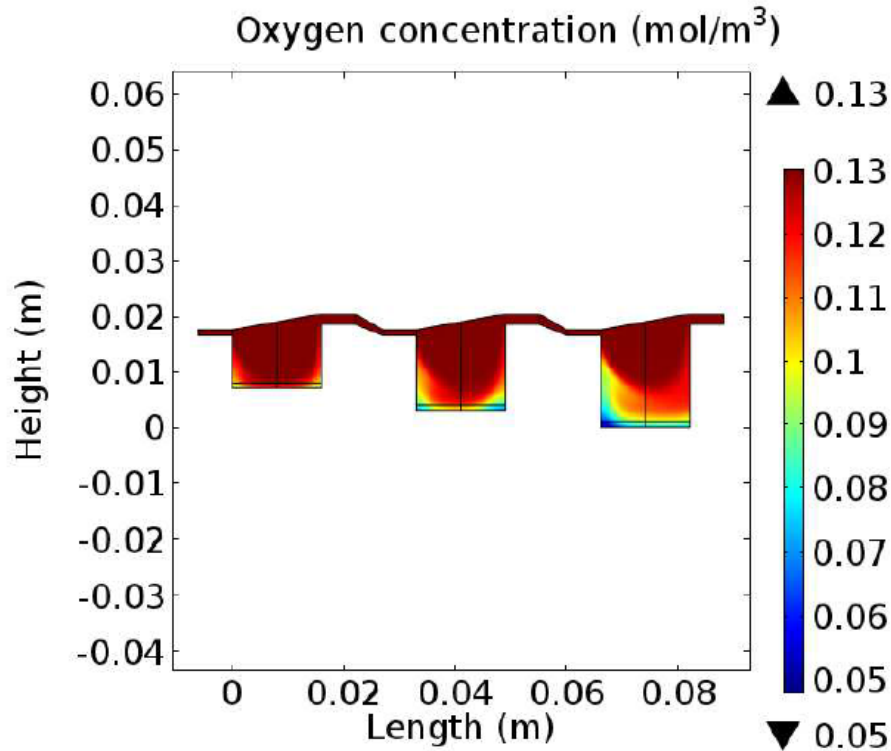
➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer in a single pot? 

➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer across multiple pots? 

➤ **Question:** can we exploit the vertical O<sub>2</sub> gradient in the pots?

# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

COMSOL 5.0.0.244

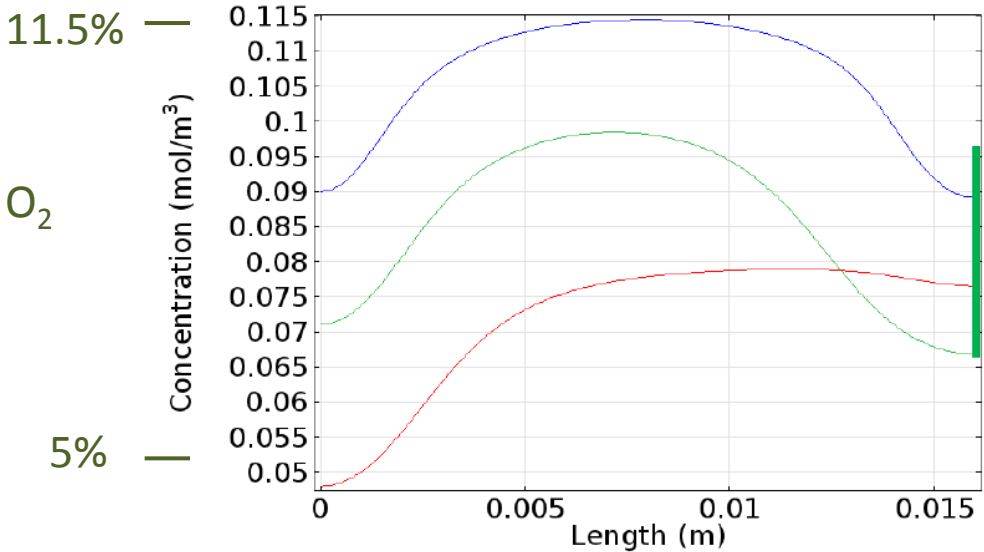


Result for  $Q = 180 \mu\text{L}/\text{min}$ . Cell surface raised by 7mm, 3mm and 1mm in pots. **Left:** O<sub>2</sub> concentration profile. **Right:** Flow profile.

# Mathematical modelling of the Kirkstall Quasi-Vivo QV900 system

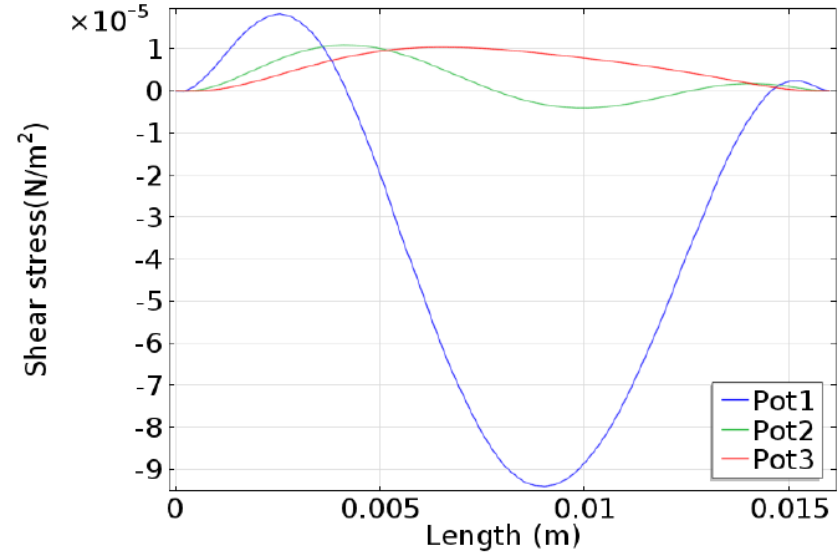
COMSOL 5.0.0.244

Oxygen concentration at cell surface




COMSOL 5.0.0.244


Shear stress at cell surface



Result for  $Q = 180 \mu\text{L}/\text{min}$ . Cell surface raised by 7mm, 3mm and 1mm in pots. **Left:**  $\text{O}_2$  concentration at the cell surface. **Right:** Shear stress at the cell surface.

**$\text{O}_2$  ranges:** pot 1, 9%-11.5%; pot 2, 7%-10%; pot 3, 5%-7.7%

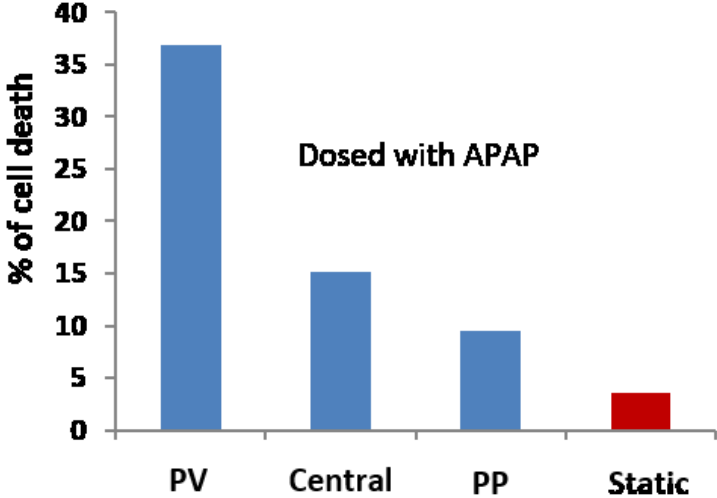
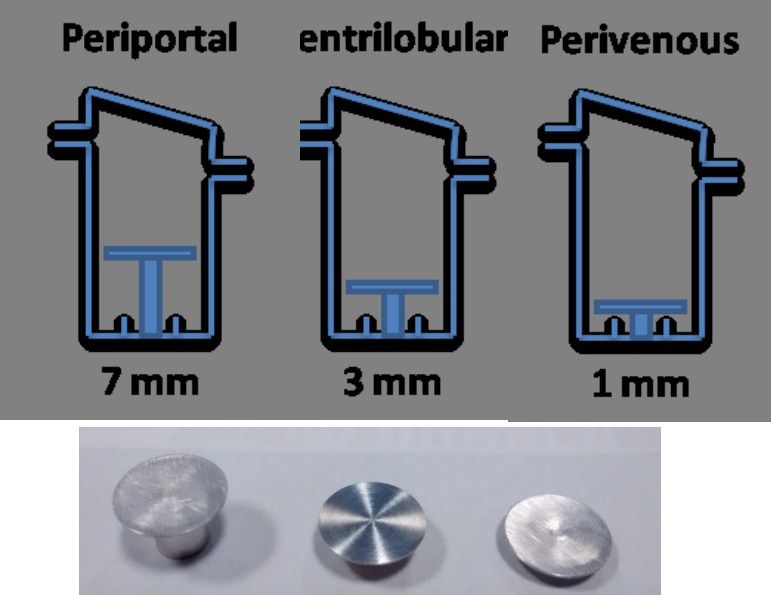
➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer in a single pot? 

➤ **Question:** can we capture an O<sub>2</sub> range of 13%-4% at the cell layer across multiple pots? 

➤ **Question:** can we exploit the vertical O<sub>2</sub> gradient in the pots? 

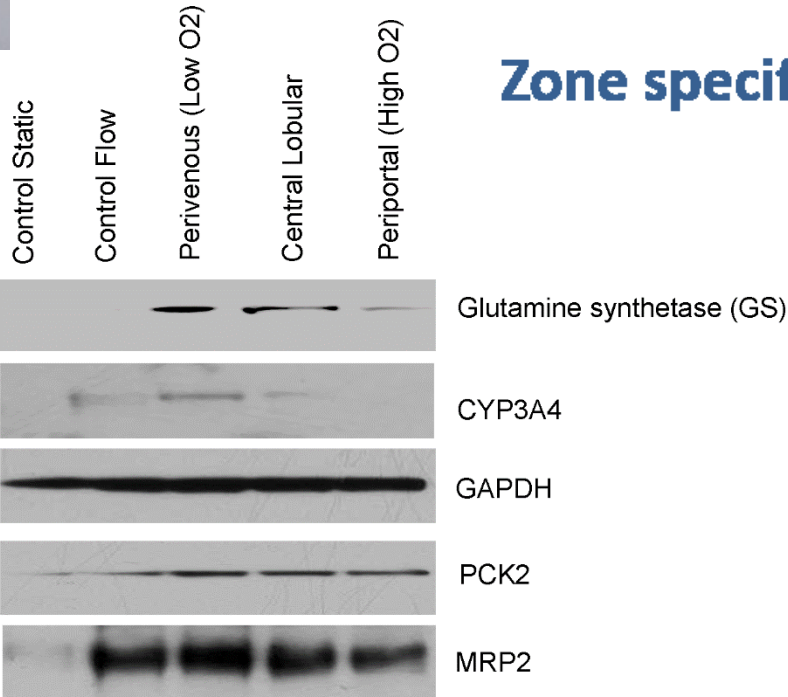
➤ **O<sub>2</sub> ranges:** pot 1, 9%-11.5%; pot 2, 7%-10%; pot 3, 5%-7.7%.

# Kirkstall QV – Zonated Liver Adaptation



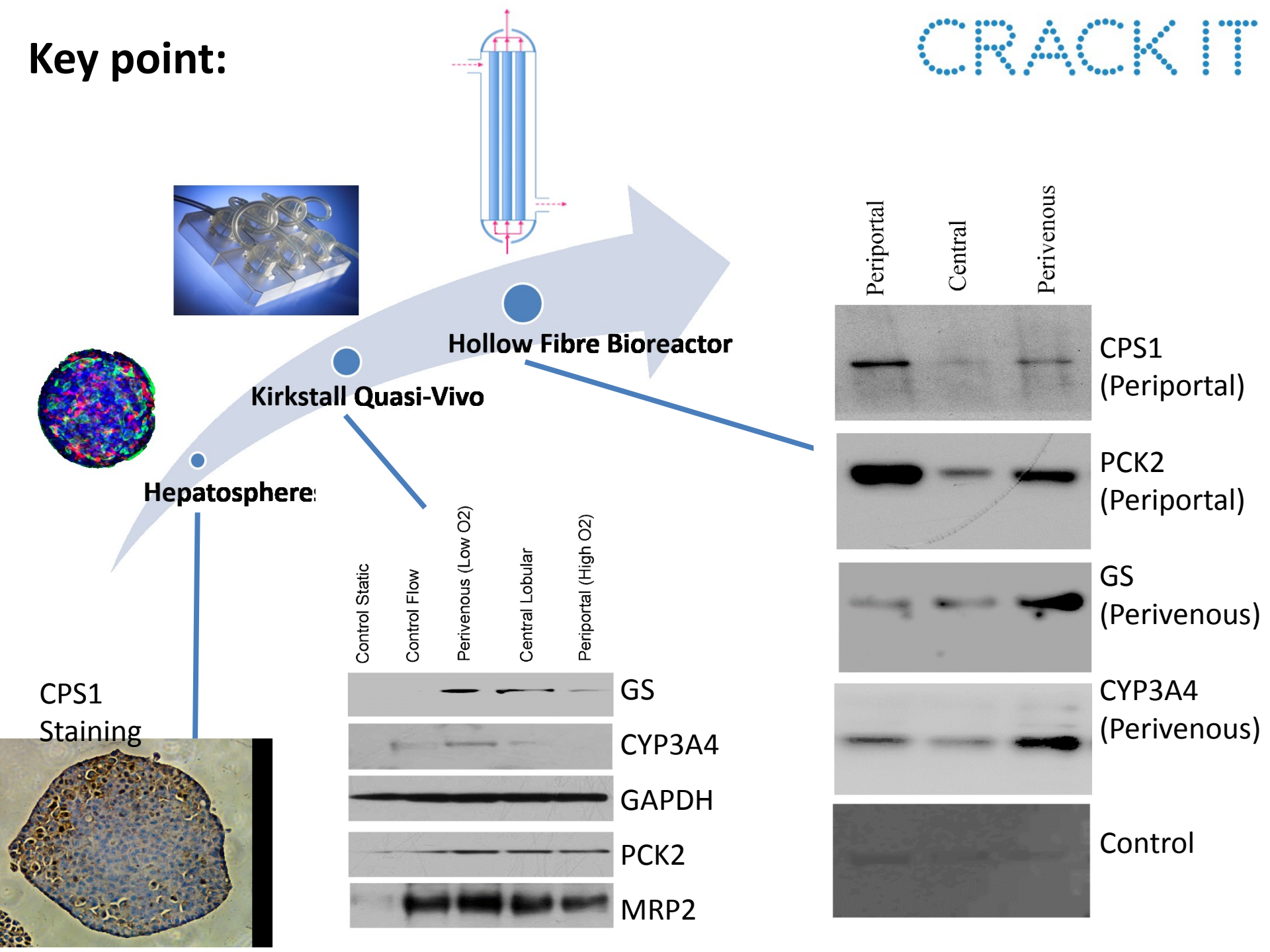
## Zone specific metabolism

**Expression of "zonation marker" proteins, following 6 days growth. Static control included.**



# Key point:

CRACK IT



Many thanks to...

CRACK IT



National Centre  
for the Replacement  
Refinement & Reduction  
of Animals in Research



James Firman



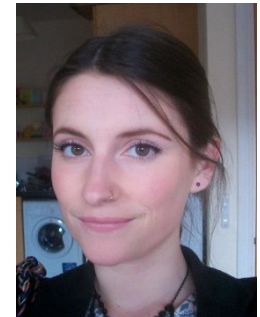
Parveen Sharma



Amy Chadwick



Joe Leedale



Harriet Gaskell



Marianne Ellis



Kim Leutchford



Rebecca Shipley



John Ward



Ian Sorrell



Sean McGinty

